

IOR Gait Overview

Acknowledgement

The IORgait is a protocol developed by the [Istituto Ortopedico Rizzoli](#) in particular, through the collaboration of [Alberto Leardini](#) and [Maria Grazia Benedetti](#)

IORgait Purpose

IORgait is a gait analysis protocol and report that is expected to be a current clinical practice. Various clinical gait analysis software is available aimed at obtaining a compromise between the following contrasting criteria:

1. Protocols for clinical gait analysis should pursue a thorough and reliable segment and joint kinematics based on subject-specific anatomical landmarks, rapid, simple, and practical procedures of data collection and reduction, particularly when children are analysed.
2. Anatomical reference frames should be defined using anatomical landmarks that be chosen to be identified easily, preferably by external palpation.
3. Report gait results using current international recommendations.

IORgait is comprised of three published protocols (described below):

1. [IORgait](#)
2. [IORfoot](#)
3. [IORtrunk](#)

The IOR protocols have been validated clinically with links to the various sections.

IORGait [Marker set](#) and associated models are described and implemented in tutorials, as detailed

IORgait

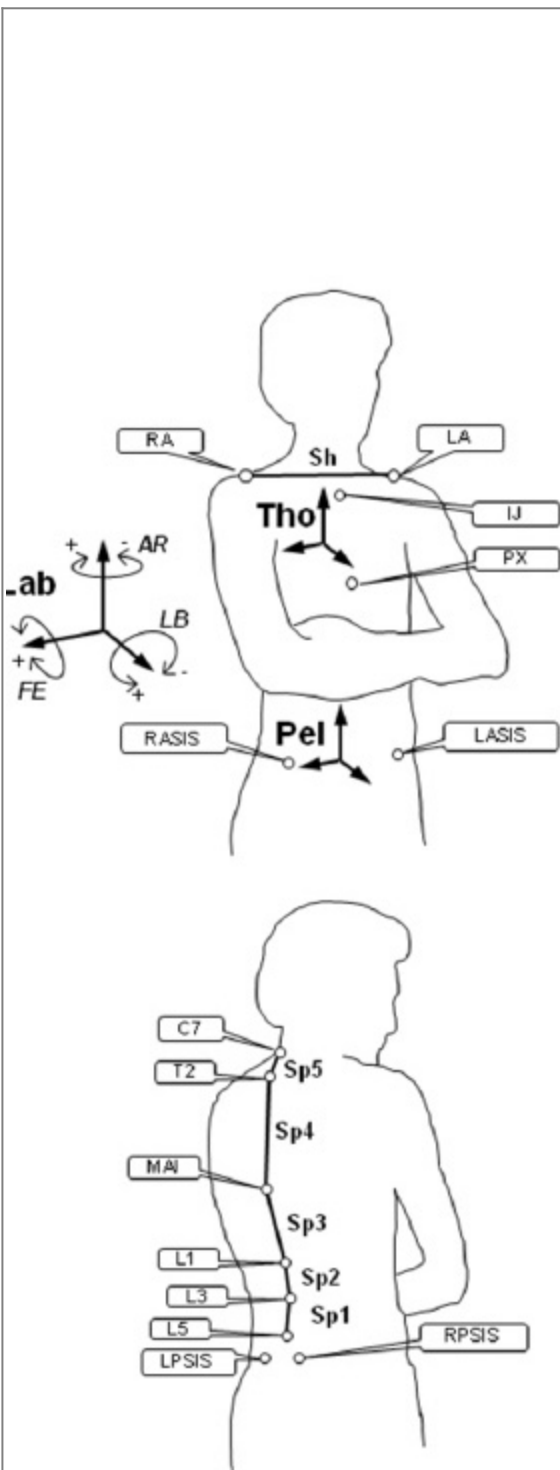
	Leardini A, Sawacha Z, Paolini G, Ingrossi N, Nativi R, Benedetti MG.(2007) A new anatomically based protocol for gait analysis in children. Gait Posture. 2007 Oct;26(4):560-71 Human movement analysis still suffers from the weakness of the currently used protocols for data collection and reduction. Reliable data collection and precise functional assessment require anatomically based definitions of the reference frames, and therefore careful identification and tracking of the landmarks. When impaired subjects are analysed, the marker-set and other measurement procedures have to be minimised to reduce the time of the experiment and ensure patient collaboration. A new protocol is proposed for the analysis of pelvis and lower limb motion, obtained as a compromise between these conflicting requirements. A marker-set is proposed which involves the attachment of 22 skin markers. The calibration by a pointer of 6 anatomical landmarks and the identification of the hip joint centre are based on a prediction approach. Anatomical reference frames and joint rotations are defined according to the recommendations. The protocol was assessed by analysing a single child in several repetitions by different examiners, and a population of 10 children, mean age 9.7-years-old. The entire analysis was repeated after subtraction of the influence of static posture angles. The minimum and maximum means of the standard deviation of five examiners of the same child were respectively 2.1 degrees in pelvic obliquity and 6.8 degrees in knee rotation. The minimum and maximum of the standard deviations from the 10 healthy children were 2.1 degrees in pelvic obliquity and 6.8 degrees in knee internal-external rotation. The protocol is feasible and allows 3D anatomical measurements of segment and joint motion, and data sharing according to current standards.
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IORfoot

	Leardini A, Benedetti MG, Berti L, Bettinelli D, Nativio R, Giannini S.(2007) Rear-foot, mid-foot and fore-foot during the stance phase of gait. Gait Posture. 2007 Mar;25(3):453- This paper proposes a new protocol designed to track a large number of segments during the stance phase with the smallest possible number of markers, with particular clinical focus on coronal plane alignment of the rear foot, transverse and sagittal plane alignment of the metatarsal bones, and changes in the medial longitudinal arch. The shape of the calcaneus, mid-foot and metatarsus were assumed to be 3D rigid bodies. The longitudinal axis of the 1st, second, third, fourth and fifth metatarsal bones and the proximal phalanx of the hallux were also tracked independently. Skin markers were placed on bony prominences or joint lines and along the course of main tendons. Trajectories of the 14 markers were collected by a high speed camera motion capture system at 120 Hz on a population of 10 young volunteers. Three-dimensional joint rotations and planar angles were calculated according to an anatomically based reference frame. The marker set was well visible throughout the stance phase of gait, even in a configuration typical of gait analysis of the full body. The time-histories of the rotations and planar angles were very repeatable among subjects and comparable with clinical and biomechanical knowledge. Several dynamic measurements were originally taken, such as elevation of the medial longitudinal arch and orientation of the metatarsal bones, rear-foot to fore-foot rotation and transverse plane deformation of the metatarsus. The information from this protocol, consistent with clinical knowledge, enhanced our understanding of the dynamics of the human foot during stance.
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For more information about other multi-segment feet, [Multi-Segmental Foot Models and Kinetic Segment Foot Models](#)

IORtrunk



Leardini A, Biagi F, Merlo A, Belvedere Benedetti MG. (2011)

Multi-segment trunk kinematics during I and elementary exercises.

[Clin Biomech \(Bristol, Avon\). 2011 Jul;26\(7\):481-9.](#)

BACKGROUND: Motion of human trunk segments in healthy subjects during activities of daily living has been described either with oversimplified models or with cumbersome techniques of isolated segments. This study describes multi-segment motion based on a new technique which represents a compromise between technical limitations of the experiments, and clinical relevance.

METHODS: The thorax segment was tracked by optimal spatial matching of four thoracic markers. The pelvis was tracked by separate bi-dimensional shoulder line rotations and translations with respect to the thorax with markers on the two acromions. Spine motion was characterised by a 5-link-segment model with additional four skin markers, in the anatomical reference frame based on four pelvic spine markers. These 14 markers were tracked in 10 healthy subjects and one clinical case during static upright standing, chair rising-sitting, step up-and-down and walking, and also during elementary flexion-extension, lateral bending, and axial rotation movements of the entire trunk.

FINDINGS: Intra-subject repeatability over multiple repetitions was found to be high for most measurements, with average standard deviation less than 1.8° for all planar rotations at the joints, and less than 1mm for shoulder translations. Motion, albeit with different patterns, was similar in all subjects, also revealing interesting coupling between the three anatomical planes.

INTERPRETATION: Considerable subject-to-subject motion occurs at each of these different segments in all three anatomical planes, during static and dynamic exercises and in motor tasks of daily living. Measurements taken with the present new model in pathological subjects shall reveal corresponding patterns and ranges of motion in abnormal conditions.

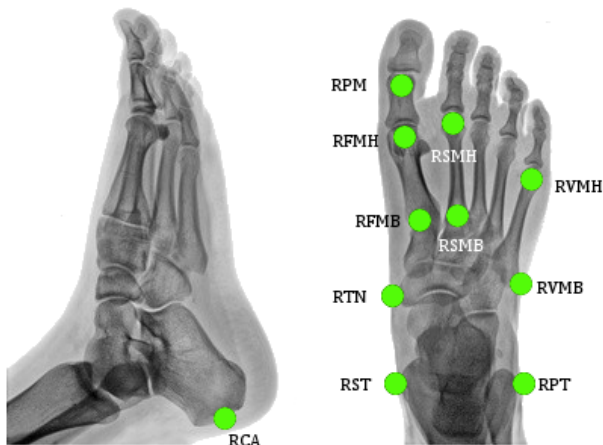
IOR Marker Sets

The [IOR Marker Sets](#) contains a detailed description of the markers that

body and foot marker sets.

A tutorial describing the IORgait model explicitly as a Visual3D model can be found [here](#)

A tutorial describing the IORgait model explicitly as a Visual3D model can be found



IOR Tutorials

The IOR Marker Set and associated models are described and implemented in detail below:

Tutorial	Description
2006 IOR Foot Model Building	Building the IOR Foot Model as described in the 2006 paper.
2007 IOR Foot Model Building	Building the IOR Foot Model to reflect updated names in the 2007 paper.
IORFoot 2014 Modifications	Building the original IOR Foot Model with all modifications from the 2014 paper.
IOR Gait Full Body Model	This tutorial explains how to implement the IOR Full Body Model. The IOR Full Body Model is a combination of the IOR Segment Trunk, and the IOR Lower Extremity Model.
IOR Gait Joint Angles	This tutorial is a continuation of the IOR Gait Full Body Model. It goes through computing different joint angles for the IOR Gait model.
IOR Gait Planar Angles	This tutorial is a continuation of the IOR Gait Full Body Model. It goes through computing planar angles with the IOR Gait model.

Repeatability

Seo SG, Lee1 DY, Moon HJ, Kim SJ, Kim J, Lee KM, Chung CY and Ch

Repeatability of a multi-segment foot model with a 15-marker set in h

[Journal of Foot and Ankle Research 2014, 7:24](#)

Background: Several 3D multi-segment foot models (MFMs) have been analysis of dynamic foot kinematics. However, reproducibility of a mo ascertained before clinical utilization of a MFM. The purpose of this s reliability of recently introduced MFM with a 15-marker set by assessi stride (intra-session) and visit-to-revisit (inter-session) repeatability.

Methods: Twenty healthy adults with a mean age of 28.9 years (10 ma tested. Three representative strides from ßve separate trials were use session. Kinematic data of foot segmental motion was collected and tr Segment Software (Motion Analysis Co., Santa Rosa, CA). A retest wa manner at an interval of 4 weeks. Coeß cients of multiple correlation (correlation coeß cient (ICC) were calculated in order to assess the int repeatability.

Results: Inter-segment foot angles from healthy adults from a MFM wi narrow range of variability during the gait cycle. The mean intra-sess which was interpreted as excellent. The mean intra-session CMC was interpreted as very good repeatability. The mean inter-session ICC wa inter-session CMC was 0.801 (–0.077), which were interpreted as exce respectively.

Conclusion: We demonstrated a MFM with a 15-marker set had high int repeatability, especially in sagittal plane motion. We thought this MFM evaluation of the segmental foot motion during gait.

Arnold JB, Mackintosh S, Jones S, Thew Risp Data (2011) of stance phase from a multi-segment foot model in people aged 50 years and older.

[Gait Posture. 2013 Jun;38\(2\):349-51..](#)

Conß dence in 3D multi-segment foot models has been limited by a lac particularly in older populations that may display unique functional fo aimed to determine the intra and inter-observer repeatability of stanc multi-segment foot model described by Leardini et al. [2] in people ag healthy adults participated (mean age 65.4 years SD 8.4). A repeated used with data collected from four testing sessions on two days from t and between-day) and inter-observer coeß cient of multiple correlation excellent similarity of stance phase joint range of motion (0.621-0.975 motion (ROM), mean diß erences (MD) between sessions were highest f for all planar ROM at the metatarsus-midfoot articulation (sagittal pla coronal plane ROM 3.9 vs. 3.1°, MD 2.3°; transverse plane ROM 6.8° v Consequently, data from the metatarsus-midfoot articulation in the 1st foot model in adults aged over 50 years needs to be considered with r study.

Deschamps K, Staes F, Bruyninckx H, Busschots E, Jaspers E, Atré A, K.(2012) Repeatability in the assessment of multi-segment foot kinema
Gait Posture. 2012 Feb;35(2):255-60.

A recently published systematic review on 3D multi-segment foot model repeatability studies providing evidence for appropriate clinical decision making. The current study was to assess the repeatability of the recently published study by Deschamps et al. [10]. Foot kinematics of six healthy adults were analyzed through two sessions including two therapists with different levels of experience and four test-retest sessions. The parameters moderate or good repeatability was observed for the within-session and between-session. A trend towards consistently higher within- and between-day repeatability was observed for the junior compared to the senior clinician. The mean inter-session variability for the 3D rotations ranged between 0.9-4.2° and 1.6-5.0° for respectively the segmental and absolute rotations, whereas for the absolute angles this variability increased to respectively 1.6-5.0° and 2.2-6.5° for the inter-therapist standard deviations ranged between 2.2° and 6.5° for the segmental rotations and between 2.8° and 7.6° for the absolute 3D rotations. The ratio of inter-therapist to intra-therapist variability ranged between 1.8 and 5.5 for the relative 3D rotations and between 1.8 and 5.5 for the absolute 3D rotations. Absolute angle representation of the planar angles was not recommended. Observations from the current study indicate that an adequate normative database is needed in gait laboratories, however, it should be stressed that experience of the examiner is crucial. Laboratories should therefore be encouraged to put effort in training the examiners.

Caravaggi P, Benedetti MG, Berti L, Leardini A. (2011)

Repeatability of a multi-segment foot protocol in adult subjects.

Gait Posture. 2011 Jan;33(1):133-5

Despite the numerous protocols for multi-segment kinematic analysis of the foot, there is scarce regarding relevant measures of reliability. The aim of the present study was to assess the inter-trial, inter-session and inter-examiner variability of one of these methods. The kinematics of the joints of the foot of two volunteers were analyzed in three sessions with different degrees of experience in three sessions, two-to-four weeks apart. For each data of five trials of level walking were collected and the rotations in the three planes between foot segments were calculated. The mean value over stance period and the standard deviation of these rotations was calculated for groups of trials according to the method described in Schwartz et al. [6]. For each rotation, the inter-examiner variability, intra-examiner variability, and the latter larger than the inter-trial. The inter-session variability was of the same order of magnitude for standard lower limb protocols for the two experienced examiners and for the inexperienced examiners.

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